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DRUG DELIVERYField of Invention

5 This invention relates to the delivery of drugs. In particular, this invention relates to the oral delivery of poorly soluble drugs using novel amphiphilic polymers with both solubilising and absorption enhancing properties.

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Background of Invention

The oral delivery of poorly soluble drugs is usually accomplished with oil based formulations such as microemulsions (Dunn, C.J., Wagstaff, A.J., Perry, C.M., Plosker, G.L., Goa, K.L., 2001, Cyclosporin - An Updated Review of the Pharmacokinetic Properties, Clinical Efficacy and Tolerability of a Microemulsion-Based Formulation Neoral R(1) in Organ Transplantation, Drugs 61: 1957 - 2016; and Porter, C.J.H., Charman, W.N., 2001, In vitro Assessment of Oral Lipid Based Formulations, Advanced Drug Delivery Reviews 50: S127-S147) or low molecular weight surface active agents (BalandraudPieri, N., Queneau P.E., Caroli Bosc, F.X., BertaultPeres, P., Montet, A.M., Durand, A., Montet, J.C. 1997, Effects of Tauroursodeoxycholate Solutions on Cyclosporin and Bioavailability in Rats, Drug Metabolism and Disposition 25: 912-916; Guo, J.X., Ping, Q.N., Chen, Y. 2001, Pharmacokinetic Behaviour of Cyclosporin A in Rabbits by Oral Administration of Lecithin Vesicle and Sandimmun Neoral, International Journal of Pharmaceutics 216: 17-21). Poorly soluble drugs are those drugs that are identified in the British Pharmacopoeia as "practically insoluble" (Medicines Commission, British Pharmacopoeia, The Stationary Office, London, 1998). Such drugs have an aqueous solubility of less than 0.1mg per millilitre of solvent (such as water) at a temperature of about 15°C - 20°C.

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Previous attempts to promote oral absorption of poorly soluble drugs such as cyclosporin, have involved

the use of oil and/or surfactant (Dunn, C.J., Wagstaff, A.J., Perry, C.M., Plosker, G.L., Goa, K.L., 2001, Cyclosporin - An Updated Review of the Pharmacokinetic Properties Clinical Efficacy and Tolerability of a  
5 Microemulsion-Based Formulation Neoral R(1) in Organ Transplantation, Drugs 61: 957 - 2016; and Porter, C.J.H., Charman, S.A., Williams, R.D., Bakalova, M.B., Charman, W.N., 1996, Evaluation of Emulsifiable Glasses for the Oral Administration of the Cyclosporin in Beagle  
10 Dogs, International Journal of Pharmaceutics 141: 227-237), bile salt (BaladraudPieri, N., Queneau, P.E., CaroliBosc F.X., BertaultPeres, P., Montet, A.M., Durand, A., Montet, J.C., 1997, Effects of Tauroursodeoxycholate Solutions on Cyclosporin and Bioavailability in Rats, Drug  
15 Metabolism and Disposition 25:912-916), phospholipid based systems (Guo, J.X., Ping, Q.N., Chen, Y., 2001, Pharmacokinetic Behaviour of Cyclosporin A In Rabbits by Oral Administration of Lecithin Vesicle and Sandimmun Neoral, International Journal of Pharmaceutics 21: 17 -  
20 21; and Leigh, M., Hoogevest, P.V., Tiemiessem, H., 2001 Optimising the Oral Bioavailability of the Poorly Water Soluble Drug Cyclosporin A Using Membrane Lipid Technology, Drug Delivery and Sciences 1: 73-77) or cyclodextrins (Miyake, K., Arima, H., Irie, T., Hirayma, F., Uekama, K., 1999, Enhanced Absorption of Cyclosporin A by Complexation with Dimethyl-Beta-Cyclodextrin in Bile duct-Cannulated and Non-Cannulated Rats, Biological and Pharmaceutical Bulletin 22: 66-72). Although a nanocapsule formed during in-situ polymerisation has also  
30 been proposed for cyclosporin delivery, this technique has difficulties in delivering the drug (Bonduelle, S., Carrier, M., Pimienta, C., Benoit, J.P., Lenaerts, B., 1996, Tissue Concentration of Nanoencapsulated Radiolabelled Cyclosporin Following Peroral Delivery in  
35 Mice or Ophthalmic Application in Rabbits, European Journal of Pharmaceutics and Biopharmaceutics, 42: 31 - 319).

Cyclosporin is a lipophilic immunosuppressant used to treat transplant and autoimmune disease patients.

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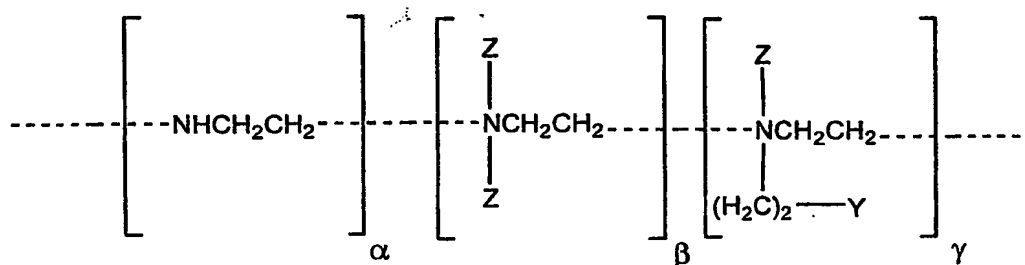
Cyclosporin is poorly soluble in a variety of solvents and is currently administered as a micro-emulsion formulation.

It is an object of embodiments of the present invention to obviate or mitigate at least one or more of the aforementioned problems.

It is a further object of embodiments of the present invention to improve delivery of poorly soluble drugs to a recipient.

### Summary of the Invention

According to a first aspect of the present invention there is provided a polyethylenimine polymer according to the following formula:



wherein  $\alpha$  is between 0 to 90%;

$\beta$  is between 0 to 100%;

$\gamma$  is between 0 to 50%;

wherein  $\alpha + \beta + \gamma = 100\%$ ; and

the Z groups are hydrophobic and are independently hydrogen or any linear or branched, substituted or unsubstituted, or cyclo form of any hydrophobic substituent; and

Y may represent a hydrophilic substituent.

It should be understood that the monomer units identified with  $\alpha$ ,  $\beta$  and  $\gamma$  may form any arrangement in the polyethylenimine polymer. The arrangement of the  $\alpha$ ,  $\beta$  and  $\gamma$  units may therefore be random or in a block copolymer form such as  $\alpha\beta\gamma\alpha\beta\gamma\alpha\beta\gamma$  etc. This is identified

above by the dashed line between the different monomer units.

The polyethylenimine polymer may be linear or branched.

5 The ratios for  $\alpha$ ,  $\beta$ ,  $\gamma$  are numerical ratios.

Typically, the Z groups may independently be selected from any of the following hydrophobic substituents: an alkyl, an alkenyl, and alkynyl, an aryl, an acyl, a hydroxy alkyl, a hydroxy acyl, polyethylene glycol or any sugar.

10 The Z groups may independently be any linear or branched, substituted or unsubstituted, or cyclo form of the following alkyl, alkenyl, alkynyl, aryl, acyl, hydroxy alkyl, hydroxy acyl, polyethylene glycol or any sugar groups:  $C_1 - C_{20}$ ;  $C_1 - C_{12}$ ;  $C_1 - C_6$  or  $C_1$ .

The Z groups may be  $C_1 - C_4$  linear alkyl groups.

Y may represent any of the following:  $-NH_2$ ;  $-NHA$ ;  $-N^+R_1R_2R_3$ ; and  $-N^+R_1R_2A$ .

20  $R_1$ ,  $R_2$ , or  $R_3$  may be selected from any of the following substituents: an alkyl, an alkenyl, an alkynyl, an aryl, an acyl, a hydroxy alkyl, a hydroxy acyl, polyethylene glycol or any sugar.

$R_1$ ,  $R_2$  and  $R_3$  may independently be any linear or branched, substituted or unsubstituted, or cyclo form of the following alkyl, alkenyl, alkynyl, aryl, acyl, hydroxy alkyl, hydroxy acyl, polyethylene glycol or any sugar groups:  $C_1 - C_{20}$ ;  $C_1 - C_{12}$ ;  $C_1 - C_6$  or  $C_1$ .

Typically,  $R_1$ ,  $R_2$  and  $R_3$  are  $C_1 - C_4$  linear alkyl groups.

30 All of  $R_1$ ,  $R_2$  and  $R_3$  may be  $CH_3$ .

Conveniently there may be between 1 and a maximum of 3 R substituents on any single nitrogen. This allows for primary, secondary and tertiary amines.

35 The groups A may be selected from any of the following linear or branched, substituted or unsubstituted, or cyclo groups:  $C_1 - C_{30}$ ;  $C_8 - C_{24}$ ; or  $C_{12} - C_{16}$ .

Typically, the groups A may be a linear  $C_{12} - C_{16}$  alkyl group.

In particular, A may be  $CH_3(CH_2)_{15}$ .

The ratio of quaternary ammonium nitrogens to  
5 nitrogens of amino groups may be selected from any of the following: 0.01% - 100%; 10% - 90%; 30% - 70%; 40% - 60%; 50% - 90% or 60% - 80%. The preferred range is 40% - 90%. A high proportion of quaternary ammonium groups promotes solubilisation of both the polyethylenimine  
10 polymer and a hydrophobic drug.

The parent polyethylenimine compound used to make the polyethylenimine polymer may have an average molecular weight of about 2 - 50kD, or more particularly, of about 10 - 25 kD.

15 The polyethylene polymer may have an average molecular weight of about 10 - 25 kD.

The polyethylenimine polymer may produce hydrophobic domains. Hydrophobic domains are areas of the molecule's self-assembly where hydrophobic compounds or compounds  
20 which are poorly soluble in water are able to reside and thus become solubilised with an aqueous disperse phase. The level of hydrophobic modification may be from 0.01 - 50%, 0.1 - 20% or 1 - 10% of amino groups. The preferred level of hydrophobic modification is 1 - 10% of amino  
25 groups.

All possible monomeric subunits in accordance with the structure as defined in formula I are shown in Figure 1:

wherein m is between 0 - 90 %;  
30 n is between 0 - 100 %;  
p is between 0 - 50 %;  
q is between 0 - 50 %;  
u is between 0 - 50 %;  
v is between 0 - 50 %;  
35 w is between 0 - 20 %;  
x is between 0 - 20 %;  
y is between 0 - 20 %; and  
z is between 0 - 20 %;

wherein,  $m + n + p + q + u + v + w + x + y + z = 100\%$ ; and

A, R<sub>1</sub>, R<sub>2</sub>, R<sub>3</sub> and Z are as defined above.

It should be appreciated that the monomer units m,  
5 n, p, q, u, v, w, x, y and z may be arranged in any order.

The ratios for m, n, p, q, u, v, w, x, y and z are numerical ratios.

Typically, if  $m = 0\%$  then n is not equal to 0%.

10 Typically, if  $n = 0\%$  then m is not equal to 0 %.

Typically, if  $p = 0\%$  then  $q + u + v + w + x + y + z$  does not equal 0%.

Typically, if  $q = 0\%$  then  $p + u + v + w + x + y + z$  does not equal 0%.

15 Typically, if  $u = 0\%$  then  $p + q + v + w + x + y + z$  does not equal 0%.

Typically, if  $v = 0\%$  then  $p + q + u + w + x + y + z$  does not equal 0%.

20 Typically, if  $w = 0\%$  then  $x + y + z + n$  does not equal 0%.

Typically, if  $x = 0\%$  then  $w + y + z + n$  does not equal 0%.

Typically, if  $y = 0\%$  then  $w + x + z + n$  does not equal 0%.

25 Typically, if  $z = 0\%$  then  $w + x + y + n$  does not equal zero.

Conveniently,  $m + n$  lies between 50 to 100%.

Conveniently,  $p + q + u + v$  lies between 20 to 50%.

30 Conveniently,  $w + x + y + z$  lies between 0.01 to 10%.

It is possible that polyethylenime may be linear ( $n=100$ ) or branched as shown in Figure 1. If  $n = 0\%$ , however, then m must be equal to a value greater than 0% as this allows for the branched material with no backbone  
35 quaternisation on erstwhile secondary amines.

It is possible that p, q, u, v, w, x, y or z may be equal to 0%. However, the sum total of p, q, u, v, w, x, y and z may be equal to a value greater than 0%, as this allows for the branched compound to be included.

Alternatively, w, x, y or z may be equal to 0%. However, the sum total of w, x, y or z may not be equal to 0%. This allows for a hydrophobically substituted branched compound.

5 Typically,  $m + n = 60\%$ ,  $w + x + y + z = 6\%$ , and  $p + q + u + v = 34\%$ . Using these ranges defines the quaternary ammonium cetyl polyethylenimine found in the Example Section of the present application.

According to a second aspect of the present  
10 invention there is provided a method of forming a polyethylenimine polymer according to the first aspect by reacting a polyethylenimine compound formed from the polymerisation of ethylenimine with a first organo halide to form an organo side chain on the polyethylenimine  
15 compound, and then a second organo halide to react with an amino group on the polyethyleneimine compound.

The polyethylenimine used may be branched or linear.

Branched polyethylenimine may be prepared by the acid catalysed polymerisation of, for example, aziridine  
20 (ethyleneimine) (Dick, C.R., Ham, G.E., J. Macromol. Sci. 1970, A4, 1301-1314; von Harpe, A., Petersen, H., Li, Y., Kissel, T., J. Control. Rel. 2000, 69, 309-332). Linear polymers may be prepared by controlling the conditions of polyethylenimine polymerisation (Zhuk, D.S., Gembitsky,  
25 P.A., Alexandrovich, A.I., US Patent No. 4,032,480).

The first organo halide may be any linear or branched, substituted or unsubstituted, or cyclo form of any alkyl, alkenyl, alkynyl, aryl or acyl halide or any hydrophilic halide. The halide may be any of fluoride,  
30 chloride, bromide or iodide.

The organo group of the first organo halide may be selected from any of the following linear or branched, substituted or unsubstituted, or cyclo groups:  $C_1 - C_{30}$ ;  $C_8 - C_{24}$ ; or  $C_{12} - C_{16}$ .

35 Typically, the first organo halide is a linear  $C_{12} - C_{16}$  alkyl halide.

In particular, the first organo halide may be cetyl bromide (e.g.  $CH_3(CH_2)_{15} Br$ ).

The second organo halide may be any alkyl, alkenyl, alkynyl, aryl or acyl halide or any hydrophilic halide. The halide may be any of fluoride, chloride, bromide or iodide.

5       The organo group of the second organo halide may be selected from any of the following linear or branched, substituted or unsubstituted, or cyclo groups:  $C_1 - C_{20}$ ;  $C_1 - C_6$ ; or  $C_1$ .

Typically, the second organo halide is a linear  $C_1 - C_6$  alkyl halide. In particular, the second organo halide  
10       may be methyl iodide.

The polyethylenimine compound and first organo halide may be mixed in an organic solvent such as tetrahydrofuran, which may then be refluxed. The  
15       refluxing may occur in an alcoholic solution of, for example, sodium hydroxide. Cetyl polyethylenimine may then be isolated and may then be reacted with the second organo halide.

The second organo halide may be added in the  
20       presence of, for example, a metal hydroxide (e.g. sodium hydroxide), a metal halide (e.g. sodium iodide) and an alcohol (e.g. methanol).

The polyethylenimine polymer may then be obtained by washing, dialysis and using an ion exchange column.

25       Further quaternisation may be obtained by adding more of the second organo halide.

The formed polyethylenimine polymer may be that as represented in Figure 1.

It is also possible to prepare a substituted linear  
30       polyethylenimine with the end nitrogens protected, subsequently deprotect the terminal amines and then attach this substituted linear polyethylenimine to the branched molecule and follow the whole conjugation step with a quaternary ammonium step.

35       According to a third aspect of the present invention there is provided a composition comprising a polyethylenimine polymer according to the first aspect and a pharmaceutically acceptable carrier.



Pharmaceutically acceptable carriers are well known to those skilled in the art and include, but are not limited to, 0.1 M and preferably 0.05 M phosphate buffer or 0.9% w/v saline. Additionally, such pharmaceutically acceptable carriers may be aqueous or non-aqueous solutions, suspensions, and emulsions. Examples of non-aqueous solvents are propylene glycol, polyethylene glycol, vegetable oils such as olive oil, and injectable organic esters such as ethyl oleate. Aqueous carriers include water, alcoholic/aqueous solutions, emulsions or suspensions, including saline and buffered media. Parenteral vehicles include sodium chloride solution, Ringer's dextrose, dextrose and sodium chloride, lactated Ringer's or fixed oils. Preservatives and other additives may also be present, such as, for example, antimicrobials, antioxidants, chelating agents, inert gases and the like.

Typically, the ratio of polyethylenimine polymer to pharmaceutically acceptable carrier ranges from any of the following: 0.0001 - 100 w.v., 0.005 - 50 w.v.; 0.001 - 30 w.v.; 0.001 - 10 w.v.; or 0.01 - 1 w.v.

According to a fourth aspect of the present invention there is provided a pharmaceutical composition comprising a polyethylenimine polymer according to the first aspect and a drug.

The drug may be poorly soluble in aqueous solvents such as water. The drug may be administered to a patient as a solution or a particulate formulation.

The drug may be selected from any of the following: cyclosporin; steroids such as prednisolone, oestradiol, testosterone; drugs with multicyclic ring structures which lack polar groups such as paclitaxel; and drugs such as etoposide.

Typically, the ratio of the polyethylenimine polymer to the drug may be selected from any of the following: 0.001 - 100%; 0.1 - 100%; 1 - 100%; 10 - 90%; 30 - 70%.

The pharmaceutical composition may also comprise a pharmaceutically acceptable carrier.

Typically, the ratio of polyethylenimine polymer to drug to pharmaceutically acceptable carrier may be in the range of 5 - 20mg : 0.5 - 5mg : 0.5 - 5mL or 5 - 20mg : 0.5 - 5mg : 0.5 - 5g. In particular, the ratio of polyethylenimine polymer to drug to pharmaceutically acceptable carrier may be about 10mg:2mg:1mL or about 10mg:2mg:2g.

The pharmaceutical composition may be in the form of any of the following: tablets, suppositories, liquid capsule, powder form, or a form suitable for pulmonary delivery.

When tablets are used for oral administration, typically used carriers include sucrose, lactose, mannitol, maltitol, dextran, corn starch, typical lubricants such as magnesium stearate, preservatives such as paraben, sorbin, antioxidants such as ascorbic acid,  $\alpha$ -tocopheral, cysteine, disintegrators or binders. When administered orally as capsules, effective diluents include lactose and dry corn starch. A liquid for oral use includes syrup, suspension, solution and emulsion, which may contain a typical inert diluent used in this field, such as water. In addition, sweeteners or flavours may be contained.

Suppositories may be prepared by admixing the compounds of the present invention with a suitable non-irritative excipient such as those that are solid at normal temperature but become liquid at the temperature in the intestine and melt in rectum to release the active ingredient, such as cocoa butter and polyethylene glycols.

The dose of the polymer can be determined on age, body weight, administration time, administration method, combination of drugs, the level of condition of which a patient is undergoing therapy, and other factors. While the daily does may vary depending on the conditions and body weight of patients, the species of active ingredient, and administration route, in the case of oral

use, the daily dose may be about 0.1 - 100 mg/person/day, preferably 0.5 - 30 mg/person/day.

According to a fifth aspect of the present invention there is provided a method of dissolving poorly soluble drugs suitable for oral delivery, using a preformed polymer.

By preformed polymer herein is meant a polymer which already exists and does not need to be formed during an in-situ polymerisation step.

The preformed polymer may be a polyethylenimine polymer according to the first aspect.

The poorly soluble drug may be selected from any of the following: cyclosporin; steroids such as prednisolone; oestradiol; testosterone; drugs with multicyclic ring structures which lack polar groups such as paclitaxel; drugs such as etoposide.

The fact that  $R_1$ ,  $R_2$ ,  $R_3$  and  $R_4$  may be long chain alkyl groups or other hydrophobic groups makes it possible for the polyethylenimine polymer according to the first aspect to dissolve poorly soluble drugs in aqueous media.

The preformed polymer may also be used to dissolve polar (aqueous soluble) materials within hydrophobic media.

According to a sixth aspect of the present invention there is provided use of a preformed polymer according to the fifth aspect in dissolving poorly soluble drugs in the preparation of a composition.

The composition may be a pharmaceutical composition comprising a drug and/or a pharmaceutically acceptable carrier.

#### **Brief Description of the Drawings**

Embodiments of the present invention will now be described, by way of example only, with reference to the accompanying drawings in which:

Figure 1 is a representation of a polyethyleneimine polymer formed according to the present invention; and

Figure 2 is a Transmission Electron Microscopy (TEM) image of quaternary ammonium cetyl polyethyleneimine (QCPEI2) and cyclosporin nanoparticles.

## 5 Examples

### Example 1 - Synthesis of Quaternary Ammonium Cetyl Polyethylenimine (QCPEI)

Alkylation of polyethylenimine was carried out according to a previously reported method (Noding, G., Heitz, W., 1998, Amphiphilic Polyethylenimines Based on Long-Chain Alkyl Bromide Macromolecular Chemistry and Physics 199: 637 - 1644). Briefly, polyethylenimine ( $M_w$  = 25kD, 5g) was alkylated by refluxing with cetyl bromide (1.8g) and tetrahydrofuran (50ml) for 48 hours, followed by the addition of an alcoholic solution of sodium hydroxide (4.8g in 25ml methanol), and a further reflux period of 24 hours. Sodium bromide was removed by filtration and the product isolated by evaporation of the solvent, exhaustive dialysis and freeze-drying. 0.6g of cetyl polyethylenimine was then quaternised by reaction with methyl iodide (2.6ml) in the presence of sodium hydroxide (0.23g), sodium iodide (0.28g) and methanol (100ml) for 3 hours at 36°C. The product was isolated by precipitation in ether (400ml), washing with ethanol, exhaustive dialysis of an ethanolic solution and elution through an ion exchange column to isolate the hydrochloride salt.

A yellow cotton wool like solid which is the quaternary ammonium cetyl polyethyleneimine (QCPEI1) was obtained on freeze drying.

A further quaternisation of quaternary ammonium cetyl polyethyleneimine (QCPEI1) produced a doubly quaternised compound, i.e. di-quaternary ammonium cetyl polyethyleneimine (QCPEI2).

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### **Characterisation of Quaternary Ammonium Cetyl Polyethylenimine**

$^1\text{H}$  NMR and  $^1\text{H}$  correlation spectroscopy as well as  $^{13}\text{C}$  NMR experiments (Bruker, AMX 400 MHz spectrometer, Bruker

Instruments UK) were carried out on the quaternary cetyl polyethyleneimine in deuterated methanol. Elemental analysis was carried out on the products using a Perkin Elmer 2400 analyser.

5

### **Polymer Aggregation**

The aggregation of an aqueous solution of the polymers was studied using a pyrene probe for hydrophobic domains (see Kalyanasundaram, K., Thomas, J.K., 1977, Environmental Effects on the Vibronic Band Intensities in Pyrene Monomer Fluorescence and the Application to Studies of Micellar Systems, Journal of the American Chemical Society 99: 2039 - 2044). Fluorescence scans (excitation = 340nm) were performed on various concentrations of the polymer dissolved in an aqueous pyrene solution (2 $\mu$ M). The ratio of the intensity of the third and first peaks ( $I_3/I_1$ ) was used to assess the hydrophobicity of the pyrene environment which is an indirect probe for polymer association.

Polymer aggregation was also assessed by recording the hypsochromic shift in the UV absorption spectrum of methyl orange (Lieske, A., Jaeger, W., 1999, Block Copolymers Containing Polysoap Blocks, Tenside Surfactants Detergents 36: 155 - 161) in 25 $\mu$ M in 0.02M borate buffer when encapsulated within a hydrophobic environment. UV absorption scans (300 - 600nm) were performed on various concentrations of the polymer dissolved in the methyl orange-borate solution and the wavelength of maximum absorbance noted.

30

**TABLE 1: Quaternary ammonium cetyl polyethyleneimine (QCPEI1) aggregation in aqueous solution as measured by the increase in ( $I_3/I_1$ ) ratio in the pyrene fluorescence and by the hypsochromic shift in the methyl orange spectra**

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QCPEI1 I3/I1 ratio (QCPEI1 concentration in mg mL <sup>-1</sup> )	QCPEI1 Methyl Orange wavelength of maximum absorbance (QCPEI1 concentration in mg mL <sup>-1</sup> )	QCPEI2 I3/I1 ratio (QCPEI2 concentration in mg mL <sup>-1</sup> )	QCPEI2 Methyl Orange wavelength of maximum absorbance (QCPEI2 concentration in mg mL <sup>-1</sup> )
0.64 (0)	465 (0)	0.61 (0)	465 (0)
0.88 (0.87)	450 (0.50)	0.823 (0.81)	456 (0.55)
0.89 (1.73)	452 (1.52)	0.862 (1.621)	450 (1.63)
0.92 (3.73)	452 (3.73)	0.871 (3.24)	458 (3.70)
0.98 (7.04)	454 (7.80)	0.853 (4.37)	455 (7.85)
		0.926 (6.49)	456 (14.25)

The synthesis of the cetyl polyethylenimine was confirmed by a proton NMR and assignments were made as follows:

5  $\delta = 0.87 = \text{CH}_3$  (cetyl),  $\delta 1.25 = \text{CH}_2$  (cetyl),  $\delta 1.45 = \text{CH}_2 - \text{N}$  (cetyl),  $\delta 2.7 - 2.8 = \text{CH}_2 - \text{N}$  (cetyl and polyethylenimine). Quaternisation of cetyl polyethylenimine to produce quaternary ammonium cetyl polyethylenimine was confirmed by <sup>13</sup>C NMR:  $\delta 14.6 =$   
 10  $\text{CH}_3$ (cetyl),  $\delta 23.9 = \text{CH}_2$ (cetyl),  $\delta 52.5$  and  $54.8 = \text{CH}_3(\text{CH}_3\text{N}^+)$ ,  $\delta 58.8$  and  $63.5 = \text{CH}_2\text{N}$  and  $\text{CH}_2\text{N}^+(\text{polyethylenimine})$  and <sup>1</sup>H NMR -  $\delta 0.90 = \text{CH}_3$  (cetyl),  $\delta 1.3 = \text{CH}_2$  (cetyl),  $\delta 1.47 = \text{CH}_2$  (cetyl),  $\delta 1.85 = \text{CH}_2 - \text{N}$  (cetyl),  $\delta 2.5 - 4.7 = \text{CH}_2\text{N}$ ,  $\text{CH}_2\text{N}^+$  and  $\text{CH}_3\text{N}^+$ .

15 The yields of cetyl polyethylenimine, quaternary polyethyleneimine (QCPEI1) and di-quaternary cetyl polyethyleneimine (QCPEI1) were 67%, 85% and 46%, respectively.

20 The degree of cetylation was found to be 5.2% of all amine groups using elemental analysis data. The degree of conversion of amines to quaternary ammonium moieties was approximately 64% for quaternary cetyl polyethylenimine and 81% for di-quaternary cetyl polyethylenimine.

25 Both quaternary ammonium polymers aggregate to produce hydrophobic domains in aqueous solution (See Table 1). This is shown by the increase in the I3/I1 values and also by the shift to a lower wavelength of the

5 methyl orange peak. These hydrophobic domains serve to solubilise poorly aqueous soluble (hydrophobic) drugs such as cyclosporin; in the case of the less quaternised variant - QCPEI1 which forms a clear micellar liquid with cyclosporin, when freshly prepared (Table 1), effectively encapsulating cyclosporin within the hydrophobic domains.

**Example 2 - Preparation of Quaternary Cetyl Polyethylenimine - Cyclosporin Formulations**

10 Quaternary cetyl polyethylenimine polymers were dissolved by probe sonication on ice (Soniprep Instruments, UK) followed by the addition of cyclosporin, which was incorporated into the polymer solution by probe sonication. Formulations were stored for up to 13 days  
15 and observed for particle formation. Particulate formations were sized by photon correlation spectroscopy, imaged by both transmission electron microscopy (TEM) with negative staining (see Wang, W., Tetley, L., Uchegbu, I.F., 2001. The Level of Hydrophobic  
20 Substitution and the Molecular Weight of Amphiphilic Poly-L-Lysine-based Polymers Strongly Affects Their Assembly into Polymeric Bilayer Vesicles, Journal of Colloid and Interface Science 237: 200-207) and freeze fracture electron microscopy (see Uchegbu, I.F., Schatzlein, A.G., Tetley, L., Gray, A.I., Sludden, J.,  
25 Siddique, S., Mosha, E., 1998, Polymeric Chitosan - Based Vesicles for Drug Delivery, Journal of Pharmacy and Pharmacology 50: 453-458). Clear micellar formulations were filtered with a 0.45µm filter and the filtered  
30 formulations assayed by HPLC using a reverse phase Waters Spherisorb ODS column (25cm x 4.6mm), eluted with a water, acetonitrile tert-butyl methyl ether, orthophosphoric acid (350:600:50:1). Detection was by UV( $\lambda$ =210nm).

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**Table 2: QCPEI-cyclosporin formulations**

Formulation	Initial Appearance	Initial Mean Particle Size (nm)	% Recovery of cyclosporin from micellar solutions(a)		Mean Particle Size (nm)	
			Freshly prepared (mean $\pm$ s.d.)	After storage (2-8°C) for 90 days (mean $\pm$ s.d.)	Storage (2-8°C) for 4 days followed by exposure to room temperature for 15 min	Storage (2-8°C) for 3 days followed by exposure to 37°C for 15 min
QCPEI1	Clear liquid	-	78.7 $\pm$ 8.14 (n=3)	93.3 $\pm$ 6.60 (n=4)	558 (n=3)	608 (n=6)
QCPEI2	Colloidal	310 (n=4)	-	-	377 (n=1)	512 (n=3)

(a) Initial Concentration = 2mg mL<sup>-1</sup>

n Denotes number of formulations assayed.

5

[In Table 2 the blank boxes (represented with a "-") represent particulate formulations, which cannot be assayed in the same way as micellar formulations].

10

As shown in Table 1 both quaternary ammonium polymers (i.e. QCPEI1 and QCPEI2) aggregate to produce hydrophobic domains in aqueous solutions. These hydrophobic domains serve to solubilise cyclosporin. In the case of the less quaternised variant - QCPEI1 forms a clear micellar liquid with cyclosporin, when freshly prepared, effectively encapsulating cyclosporin within hydrophobic domains. However, as shown in Table 2, the polymer exhibits a lower critical solution temperature and becomes less hydrated with increase in temperature resulting in aggregation of the polymeric micelles to form nanoparticles. Furthermore, Table 2 shows storage of QCPEI1 at refrigeration temperature preserved the micellar formulation. The micellar formulation is preserved as analysis of the optically clear samples after storage for 90 days shows that there is no precipitation of cyclosporin.

25

In contrast to QCPEI1, the doubly quaternised compound QCPEI2, which is less water soluble than QCPEI1



initially formed stable nanoparticles with cyclosporin. Figure 2 shows that the double quaternarised compound (QCPEI2) does not form micelles with cyclosporin. The size bar shows that the aggregates formed are too large to be micelles although the image could show an aggregate of lots of micelles. These will still be technically nanoparticles as the formulation is not optically clear.

Although the polymer forms micelles within which cyclosporin is solubilised, the polymer exhibits a lower critical solution temperature and becomes less hydrated with increase in temperature resulting in aggregation of the polymeric micelles to form nanoparticles after exposure to elevated temperatures (i.e. removal from the fridge, Table 2). However, storage of QCPEI1 at refrigeration temperature preserved the micellar formulation (Table 2) and there was no conversion of the micelles into nanoparticles. In contrast to QCPEI1, the doubly quaternised compound QCPEI2, which is less water soluble than QCPEI1, initially formed stable nanoparticles with cyclosporin (Figure 2, Table 2) and does not form the micelles with cyclosporin.

### **Example 3 - Oral Administration of Quaternary Cetyl Polyethylenimine-Cyclosporin Formulations**

Groups of male Wistar rats (n=4 i.e. the group size, weight = 200 - 220g) were fasted for 12 hours before dosing and subsequently dosed intragastrically (10mg kg<sup>-1</sup>) with an optically clear quaternary cetyl polyethylenimine (QCPEI1) - cyclosporin formulation (10:2); a particulate quaternary cetyl polyethylenimine (QCPEI2) - Cyclosporin (10:2) formulation; Neoral (Registered Trademark) or water. Neoral is a microemulsion formulation of cyclosporin manufactured and marketed by Novartis.

Blood was taken from the tail vein of these anaesthetised rats at 1 hour, 4 hours and 24 hours after dosing. Plasma was separated by centrifugation at 1000g and stored at -20°C until analysis could be performed on the samples. Cyclosporin was measured in the plasma samples using a monoclonal antibody radioimmunoassay kit

(Cyclo-Trac SP-Whole Body Radioimmunoassay Kit) supplied by Diasorin, UK.

**Table 3: Blood Levels Following Oral Cyclosporin Dosing**

Time	Formulations ngL <sup>-1</sup> of cyclosporin in blood		
	Neoral ®	QCPEI1	QCPEI2
1h	1525±267*	583±284	748±482
4h	1521±163	1179±360	1387±539
24h	346±37	315±95	295±45

5

\* = statistically significant difference between groups at the same time point (p<0.05)

10 The oral QCPEI1 formulations were well tolerated in rats with no gross adverse events recorded. Plasma levels at the 4 hour time point from the oil free QCPEI formulations were indistinguishable from peak levels obtained using Neoral (Registered Trademark), although Neoral (Registered Trademark) was absorbed faster than 15 the QCPEI formulations shown in Table 3. The amphiphilic polyethyleneimine polymer therefore promotes the absorption of a poorly soluble drug such as cyclosporin.

20 Within the 37°C environment of the gut lumen it is assumed, although not wishing to be bound by theory, that the narrow particle formulation prevails for both polymers and that these nanoparticles experience the gradual loss of cationic micellar aggregates still encapsulating their hydrophobic payload. As cationic polymers are known to facilitate transport across 25 epithelial membranes and across cell membranes, these micellar aggregates may also facilitate the intestinal absorption of cyclosporin. The disassociation of the nanoparticle into single micellar aggregates results in the delayed absorption when compared to the oil 30 containing formulation.

**Example 4 - Oral Delivery of Cyclosporin 2**

This Example examines the effect of intermediate and low molecular weight quaternary ammonium hexadecyl polyethylenimine on the oral delivery of cyclosporine A.

**Materials**

Polyethylenimine (Mw = 10kD) was supplied by Polysciences, UK. Polyethylenimine (Mw = 1.8kD), hexadecyl bromide, methyl iodide and sodium iodide were all obtained from Sigma-Aldrich, Co., UK. Ethanol, diethyl ether and tetrahydrofuran were supplied by the Department of Pure and Applied Chemistry, University of Strathclyde.

15

**Methods**

Intermediate molecular weight quaternary ammonium cetyl PEI with two different levels of quaternary ammonium modification (Q1<sub>10</sub> and Q2<sub>10</sub>) were synthesised by reacting polyethylenimine (PEI, Mw = 10kD) with both cetyl bromide and methyl iodide as described for QCPEI1 and QCPEI2 respectively in Example 1. Low molecular weight quaternary ammonium cetyl PEI with a high level of quaternary ammonium modification (Q2<sub>1.8</sub>) was synthesised by reaction of PEI (Mw = 1.8kD) with both cetyl bromide and methyl iodide as described for QCPEI2 in Example 1. Q1<sub>10</sub>, Q2<sub>10</sub>, and Q2<sub>1.8</sub> cyclosporine (2mg mL<sup>-1</sup>) formulations, each containing 10mg mL<sup>-1</sup> of the respective amphiphilic PEI were prepared as described in Example 2.

Male Wistar rats (mean weight = XXg [WPC PLEASE COMPLETE], n = 4) were dosed orally with QCPEI1, Q1<sub>10</sub>, Q2<sub>10</sub> or Neoral formulations of cyclosporine (7.5mg kg<sup>-1</sup>).

Blood was then sampled at various time intervals and cyclosporine analysed in the sampled blood using the radioimmunoassay procedure described in Example 3. In a separate experiment male Wistar rats (mean weight = XXg [WPC PLEASE COMPLETE], n = 4) were dosed orally with Q2<sub>10</sub>, Q2<sub>1.8</sub>, or Neoral formulations of cyclosporine (10mg kg<sup>-1</sup>). A further group was dosed with a dispersion of cyclosporine (10mg kg<sup>-1</sup>) in water which was shaken just prior to administration. Blood was sampled from these 4 groups of animals at various time intervals and cyclosporine analysed in blood using the radioimmunoassay procedure described in Example 3.

### Results

**Table 4: Blood levels of cyclosporine after dosing animals orally with 7.5mg Kg<sup>-1</sup> cyclosporine**

Formulation	Blood levels (ng mL <sup>-1</sup> , n = 4, mean ± s.d.)		
	1h	4h	24h
Q1 <sub>10</sub>	615 ± 351*	854 ± 376	73 ± 38
Q2 <sub>10</sub>	1050 ± 456	1163 ± 326	95 ± 19
QCPEI1	576 ± 320*	799 ± 481	84 ± 44
Neoral	1496 ± 447	989 ± 301	150 ± 68

\*Statistically significantly different from Neoral (p < 0.05)

**Table 5: Blood levels of cyclosporine after dosing animals orally with 10mg Kg<sup>-1</sup> cyclosporine**

Formulation	Blood levels (ng mL <sup>-1</sup> , n = 4, mean ± s.d.)		
	1h	4h	24h
Q2 <sub>1.8</sub>	889 ± 336*	1677 ± 840	461 ± 153 <sup>#</sup>
Q2 <sub>10</sub>	1213 ± 196* #	1865 ± 516 <sup>#</sup>	565 ± 115 <sup>#</sup>
Cyclosporine dispersion in water	439 ± 345*	617 ± 277*	88 ± 43
Neoral	2026 ± 209 <sup>#</sup>	1915 ± 158 <sup>#</sup>	475 ± 133 <sup>#</sup>

\*Statistically significantly different from Neoral (p < 0.05).  
 5       <sup>#</sup>statistically significantly different from cyclosporine dispersion in water.

#### **Comment on Results**

At the 7.5mg kg<sup>-1</sup> dose level Q2<sub>10</sub> had an equivalent  
 10 bioavailability with Neoral while Q1<sub>10</sub> and QCPEI1 delivered less cyclosporine via the oral route after 1h when compared to Neoral, although cyclosporine levels equivalent to Neoral were delivered at the 4h and 24h time points by both Q1<sub>10</sub> and QCPEI1.

At the 10mg kg<sup>-1</sup> dose level, all formulations  
 15 delivered less cyclosporine than Neoral at the 1h time point although Q2<sub>10</sub> improved the absorption of cyclosporine when compared to cyclosporine dispersion in water. At the 4h time point both Q2<sub>10</sub> and Q2<sub>1.8</sub> were  
 20 bioequivalent with Neoral whereas due to the high standard deviations obtained with Q2<sub>1.8</sub>, this formulation was statistically indistinguishable from the cyclosporine

dispersion in water. At the 24h time point all formulations resulted in a greater absorption of cyclosporine when compared to the cyclosporine dispersion in water.

- 5 It is clear that polyethylenimine amphiphiles are able to promote the absorption of cyclosporine.

### **Example 5: Stability of Cyclosporin Solutions**

This Example relates to assessing the stability of  
10 quaternary ammonium polyethylenimine - cyclosporine formulations.

#### **Materials**

Polyethylenimine (Mw = 10kD) was supplied by  
15 Polysciences, UK. Polyethylenimine (MW = 25kD), hexadecyl bromide, methyl iodide and sodium iodide were all obtained from Sigma-Aldrich, Co., UK. Ethanol, diethyl ether and tetrahydrofuran were supplied by the Department of Pure and Applied Chemistry, University of  
20 Strathclyde.

#### **Methods**

Q1<sub>10</sub> was synthesised by reacting polyethylenimine (PEI, Mw = 10kD) with both cetyl bromide and methyl  
25 iodide as described for QCPEI1 in Example 1. QCPEI1 was also synthesised as described in Example 1. Q1<sub>10</sub> and QCPEI1 Formulations of cyclosporine (2mg mL<sup>-1</sup>) containing 10mg mL<sup>-1</sup> of the amphiphilic PEIs were prepared as described in Example 2.

30 Formulations were then stored in stoppered glass containers at refrigeration temperature (2 - 8°C). At

various time intervals aliquots were sampled, filtered through a 0.45µm filter and analysed by high performance liquid chromatography (HPLC). Filtered cyclosporine samples (20µL) dissolved in acetonitrile, water (1: 1) were injected onto a Waters Spherisorb 5µm, 4.6mm X 250mm column (Waters Instruments, UK) maintained at 80°C with a Jones Chromatography Column Heater model 7971 by means of a Waters 717 autosampler and a Waters 515 isocratic pump. The mobile phase was acetonitrile: water: *tert*-butyl-methyl-ether: phosphoric acid (600:350:50:1) at a flow rate of 1.2mL min<sup>-1</sup>. Peak detection was via a Waters 486 variable wavelength UV detector with the wavelength set at 210nm and data was collected using a Waters 746 data module. A standard curve was prepared using solutions of the drug (1 - 10µg mL<sup>-1</sup>).

### Results

Time Point (days)	QCPEI1	Q1 <sub>10</sub>
0	78.7 ± 8.1	80.7 ± 17.7
7	84.6 ± 3.1	74.0 ± 8.1
41	93.7 ± 8.8	81.9 ± 3.6
109	91.0 ± 6.3	79.0 ± 0.6
181	84.4 ± 2.9	82.0 ± 2.3
281	89.4 ± 0.42	79.0 ± 1.4

### Comment on Results

Over a 9 month period the level of cyclosporine recovered from amphiphilic PEI formulations Q1<sub>10</sub> and QCPEI1 did not differ appreciably from the original levels, indicating that these formulations were stable when stored for 9 months at refrigeration temperatures.